

## FRACTURE HEALING, THE DIAMOND CONCEPT UNDER THE SCOPE: HYDROXYAPATITE AND THE HEXAGON

FRANCISCO RODRIGUEZ-FONTAN<sup>1-3</sup>

<sup>1</sup>Department of Orthopedics, University of Colorado, Anschutz Medical Campus, Aurora, Colorado, USA, <sup>2</sup>Colorado Program for Musculoskeletal Research, Department of Orthopedics, University of Colorado Anschutz Medical Campus, Aurora, Colorado, USA, <sup>3</sup>Facultad de Medicina, Universidad de Buenos Aires, Buenos Aires, Argentina

**Abstract** Bone healing after a fracture has many intercalated steps that depend on the host, type of injury, and often the orthopedist. The diamond concept since 2007 has outlined 4 main facets that have to be considered as a model by the treating surgeon at the time of injury and when nonunion develops: osteogenic cells, osteoconductive scaffolds, osteoinduction, and the biomechanical environment. All of these foment fracture healing in optimal circumstances. Yet, this work proposes other facets, such as osteoimmunology and vascularity, to be considered as well in the model. These are as important as the original four, though their correlation to the original work has been less noted until more recent literature. The mindset of the orthopedist must thoroughly analyze all these facets and many more when dealing with nonunion. This work presents, probably the most significant ones, parting from the original 4-corner diamond model and expanding it to a more representative hexagon integrated model. Metaphorically, just like the strongest inorganic constituent of the bone: hydroxyapatite.

**Key words:** bone healing, hydroxyapatite, diamond, hexagon, osteoimmunology, vascularity

**Resumen** *Consolidación de fractura, una mirada al concepto diamante: Hidroxiapatita y el hexágono*

Hay múltiples pasos intercalados en la consolidación de la fractura que dependen del paciente, el tipo de fractura y frecuentemente del ortopedista. Desde su introducción en el año 2007, el concepto del diamante ha delineado 4 facetas o aristas principales que se han de tener en cuenta por el ortopedista en el momento de la lesión y cuando la no-unión de fractura ocurre: células osteogénicas, matrices osteoconductoras, osteoinducción, y el ambiente biomecánico. Otras facetas para tener en cuenta, no menos importantes, son la osteoimmunología y la vascularidad. Estas son tan importantes como las 4 facetas originales, pero la correlación entre las mismas ha sido poco notada o integrada hasta ahora. El ortopedista tratante debe analizar todas ellas en profundidad, especialmente cuando se trata de una no-unión. Este trabajo presenta las más significantes, partiendo del modelo original del diamante de 4 facetas hacia uno más representativo e integrado como el hexágono. Metafóricamente, como el elemento inorgánico más abundante y fuerte en el hueso: la hidroxiapatita.

**Palabras clave:** consolidación de fractura, hidroxiapatita, diamante, hexágono, osteoimmunología, vascularidad

### KEY POINTS Current knowledge

- Fracture healing and nonunion management is conceptually understood as the diamond: osteogenic, osteoinductive, osteoconductive, and biomechanical. It was introduced in 2007 and has gained popularity and utility. Hydroxyapatite is the most abundant and strongest component in bone.

### Contribution to the current knowledge

- This article highlights other facets in fracture healing that lead to a 6-facet diamond with the inclusion of osteoimmunology and vascularity, mirroring the hydroxyapatite strong constitution.

Bone structure dynamically responds to common daily basic loading and straining activities (e.g., walking, running, swimming) and in extreme circumstances such as trauma (i.e., fractures), tumors, and surgery. The capacity to respond and heal is finely tuned and reflected by its natural composition: residing cells (e.g., osteoblasts, osteocytes, osteoclasts, progenitor cells) and extracellular matrix<sup>1</sup>. Of note, the extracellular matrix is constituted of approximately 40% organic (e.g., collagens, and non-collagenous proteins) and 60% inorganic matrix, which major inorganic constituent is hydroxyapatite (HA,  $\text{Ca}_5(\text{PO}_4)_3\text{OH}$ ), providing compressive strength<sup>1-3</sup>. Non-collagenous proteins allow biomineralization, while the collagen provides the structured template for hydroxyapatite deposition<sup>1,4</sup>. From a chemical perspective, hydroxyapatite is structurally an hexagon<sup>2,3,5-7</sup>. It has been widely studied and implemented in many orthopaedic procedures and implants due to its bioactive profile<sup>5,7-12</sup>.

The fracture healing, from a secondary healing perspective, can be schematically divided into three overlapping biological phases: inflammatory, repair, and remodeling. This involves intramembranous and endochondral ossification mechanisms of bone formation, which is determined by fracture gap and strain<sup>13</sup>. Giannoudis et al work, entitled "Fracture healing: The diamond concept", has transcended the vast literature gaining recognition in such appreciation of fracture healing and setting a model or template for understanding fracture healing phenomenon and for the management of nonunion (up to 10% of all fractures)<sup>14</sup>. It has received wide acceptance in the orthopaedic world as a framework for analysis of nonunions and as a decision-making tool when planning multifaceted interventions, more so in the setting of significant bone defects or recalcitrant nonunions. This 4-corner work is conceptually framing bone healing as a "diamond" by osteogenic cells (i.e., mesenchymal cells, progenitor cells), an osteoconductive scaffold (i.e., grafts, synthetic fillers), growth factors (i.e., osteoinductive cytokines) and

lastly the biomechanical environment (i.e., strain, stability, cellular mechanoreceptors)<sup>12, 15-18</sup>. The aforementioned conceptual frame of bone healing and nonunion treatment called the "diamond" concept comes short in reality and does have a number of additional facets to the original four that are worth mentioning, such as vascularity of the zone of injury, the containment of the graft, the timing of intervention, the profile of the patient (i.e., age, comorbidities, immune system) and surgical technique<sup>17</sup>.

The diamonds *per-se* have multiple facets, corners, and edges, and they can be represented by many polygons in nature. Probably, the strongest shape is the hexagon due to its mechanical strength and stability, just like the hydroxyapatite in bone<sup>19-22</sup>. Various structures, correspondingly the hexagon (e.g., honeycombs), in nature are not a coincidence and have inspired mankind to replicate in engineering due to their structural stability and reliability<sup>23</sup>.

Though from basic science knowledge advancement in the case of osteoimmunology and procedural practice in the case of vascularity; these facets seem individual factors, other than part of the whole fracture healing "diamond" concept. Hence, this work outlines these two other facets that should be integrated and recognized into the conceptual framework "diamond" model when treating fractures. This work will not delve into types of nonunion, nor infection, or patient comorbidities that oftentimes compromise fracture healing<sup>17</sup>. This article will provide an overview of the original 4 facets of the "diamond" model, and will explore more in-depth the proposed ones that configure an hexagon<sup>14</sup>.

## The four-facet diamond

### Biomechanical environment

Strain is a relative measure of deformation an object has in response to loading and is influenced by stability. In the clinical setting, stability at the fracture surfaces is the degree of load-dependent displacement<sup>16</sup>. When a fracture occurs, the load transmission is affected, the hematoma fills the gap and eventual callus formation takes place. The degree of motion at the fracture surfaces will determine the strain and is fundamental for primary or secondary bone healing<sup>17</sup>. Primary bone healing occurs where there is absolute stability, defined as bone surface contact < 0.15 mm or strain < 2%. It occurs primarily as intramembranous ossification and can be seen in non-displaced fractures or with anatomic reduction and fixation techniques (e.g., compression plate, lag screws)<sup>15</sup>. Secondary bone healing occurs with relative stability and occurs primarily as endochondral ossification. The initial strain tolerance can be around 100%, but as the callus matures and calcifies the contact area increases, and motion at the fracture decreases, then becoming around

2-10% which is tolerable for healing<sup>17</sup>. It can be seen in comminuted or displaced unstable fractures, with splinting or casting, or with non-rigid fixation techniques (e.g., bridge plating, intramedullary nailing)<sup>17</sup>. If the strain falls outside that range, fracture healing is hampered and may lead to delayed healing or nonunion<sup>17</sup>. The progenitor/stem cells and residing bone cells (i.e., osteoblasts, osteoclasts) through mechanosensation and mechanotransduction sense and respond to mechanical conditions determining their proliferation and the secretion of cytokines and enzymes<sup>24</sup>. Under appropriate mechanical stimuli stem cells can undergo chondrogenic or osteogenic differentiation while osteoblasts and osteoclasts tailor the bone resorption/reconstruction balance<sup>25</sup>. Moreover, in the setting of osteosynthesis, if implant loosening and instability take place, component wear and abrasions can stimulate macrophages and osteoblasts towards a pro-inflammatory and pro-osteolytic activity<sup>26</sup>.

### **Osteogenic cells**

At the fracture hematoma, the advent of neighboring or local progenitor and stem cells (i.e., from the periosteum, bone marrow, muscle) responds to the extracellular matrix debris, growth factors, and cytokines<sup>15</sup>. This parallel to an initial inflammatory process leads to a progenitor/stem cell proliferative response. There is a concomitant increased vascular permeability that allows more stem and immune cell chemotaxis. The fibrin matrix is progressively replaced by a forming callus due to fibroblasts and osteoclasts. The stem cells found in the callus, depending on the cytokine profile, mechanical strain, and oxygen tension of the environment will proliferate and differentiate into osteoblasts [bone morphogenetic protein (BMP), lower strain and higher oxygen tension] or chondrocytes (higher strain and lower oxygen tension)<sup>25</sup>. This results in a combination of a peripheral or cortical hard callus tissue (e.g., osteoblasts and collagen I) of predominant intramembranous ossification, and a central or medullary soft callus (chondrocytes and collagen II) of predominant endochondral ossification<sup>15</sup>.

### **Osteoconductive scaffold**

Naturally, the extracellular matrix provides an environment for cell adhesion, migration, and cues for osteogenic cells. However, when there is a significant gap and impending nonunion, some procedures can be performed to overcome this deficiency: autograft, allograft, vascularized bone graft, and Masquelet membrane, among others<sup>17</sup>. An ideal bone graft has high osteoconductivity, high osteoinductivity, and high osteogenicity; due to retained structure, and residing factors and cells<sup>27,28</sup>. Autologous bone grafts remain the gold standard material as it minimizes the risk for rejection and provides a highly osteoconductive and osteoinductive environment (e.g., iliac crest). Notwithstand-

ing, autografts have significant disadvantages: donor-site morbidity, risk of infection, potential nerve damage, and increased blood loss due to the longer surgical time and reimplantation of the graft<sup>28,29</sup>. Further, autograft supply is limited in cases of large bone defects and is ultimately not a feasible option for patients with poor bone quality (i.e., osteoporosis). These disadvantages have led to the increased use of cadaveric bone allografts<sup>27</sup>. These undergo rigorous preparation and the processed bone lacks osteogenic cells and has limited growth factors, which may lead to graft failure<sup>27,30</sup>. Indeed, low osteoconductivity and low osteoinductivity of commercially available allografts have been reported as reasons for failure in animal models of spinal fusion<sup>31</sup>. To overcome this limitation and enhance stable bone formation and fusion, there has been an interest in developing biologic adjuvant therapies for allografts or graft alternatives such as growth factor supplementation and/or adding osteoprogenitor cells<sup>32,33</sup>. Regarding graft alternatives, such as synthetic grafts (e.g., coralline, silicate ceramic, tricalcium phosphate), mimic the mineral portion of bone but cannot provide an optimal healing environment<sup>27</sup>. However, the demineralized bone matrix alternative is an allograft-derived substance containing primarily collagen I and BMPs, hence is both osteoconductive and osteoinductive in the presence of progenitor cells<sup>27</sup>.

### **Osteoinduction**

As the fracture hematoma develops, a vast repertoire of signaling molecules such as interleukins (IL) and growth factors are spilled locally and systemically. They are secreted by platelets, macrophages, stem cells, chondrocytes, fibroblasts, osteoblasts, and endothelial cells<sup>14</sup>. These factors initiate and orchestrate cellular events in the healing environment. They guide stem cell proliferation and differentiation. Though multiple cells secrete these factors, they are extremely intertwined in the "stem-immune" cell cross-talk defined below<sup>26,34</sup>. The most remarkable factors that promote osteogenesis are insulin-like growth factor (IGF), fibroblast growth factor (FGF), platelet-derived growth factor (PDGF), and transforming growth factor-beta (TGF $\beta$ ). The latter includes BMPs<sup>35</sup>.

### **Towards the hexagon**

#### **Osteoimmunology**

The role of immunology in the bone microenvironment can be often overlooked. It has become an entity by itself but in extreme relationship with other factors. Bone is in a constant dynamic process of resorption and reabsorption, in which maximum magnitude of expression could be

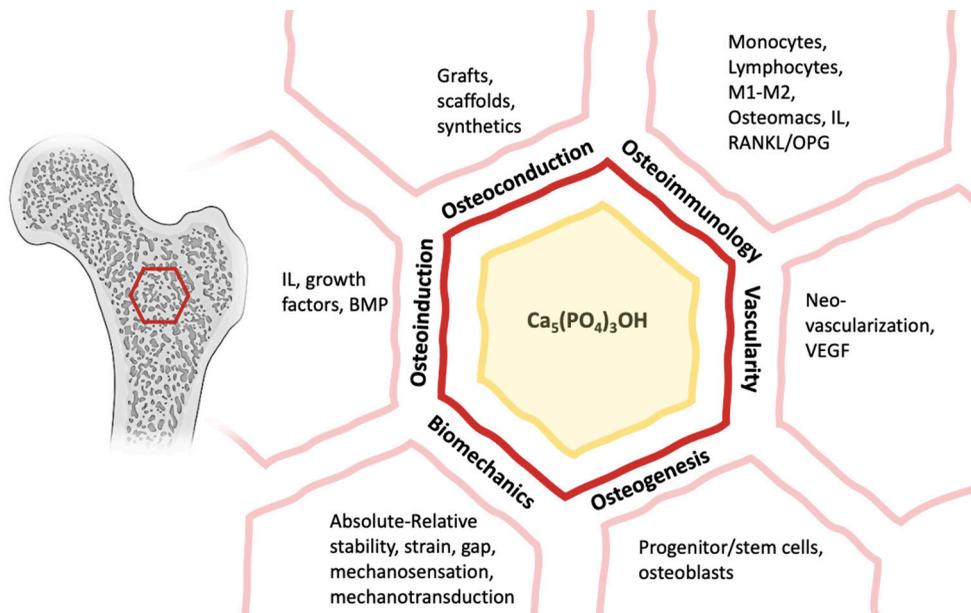
reflected by the fracture and its healing phases. Both, the immune system and bone remodeling cells are intertwined in a cross-talk that regulates each other, termed osteoimmunology by Arron and Choi (Figure 1)<sup>26,36,37</sup>. The fracture leads to the formation of hematoma which temporarily acts as a scaffold or matrix rich in cytokines, immune cells, and progenitor cells<sup>38</sup>. Polymorphonuclear cells are the first to intervene in a stepwise fashion followed by macrophages and lymphocytes. These secrete chemokines [i.e., IL-1, IL-6, IL-10, alpha tumor necrosis factor (TNF $\alpha$ ), monocyte chemoattractant protein 1 (MCP-1), alpha chemokine CXC ligand-1 (CXCL-1 $\alpha$ ), macrophage inflammatory protein 1 (MIP-1)] that attract and activate monocytes and macrophages<sup>34</sup>. The Osteomacs are residing peri-fracture macrophages that take a quick participatory influence in initiating intramembranous ossification; whereas inflammatory macrophages are those recruited during endochondral ossification<sup>13</sup>. In addition, from a phenotypic perspective, two different types of macrophages have been identified. Although it represents a simplistic bipolar manner, and more types have been recognized, M1 and M2 represent an antagonistic though necessary interaction for proper healing, which is also present in other tissues<sup>34</sup>. M1 has a predominant inflammatory action and secretes pro-inflammatory cytokines (i.e., IL-1, IL-6, TNF $\alpha$ , MCP-1) and aids in clearing debris, while M2 has a predominant anti-inflammatory effect [i.e., IL-10, TGF $\beta$ , BMP2, vascular endothelial growth factor (VEGF)], enhance mesenchymal cell recruitment and lead to regeneration<sup>13,26,34,39</sup>. The receptor activator of nuclear factor Kappa

ligand (RANKL) - osteoprotegerin (OPG) signaling axis is fundamental in osteoclastogenesis and the inflammatory or anti-inflammatory cytokine profile will modulate bone resorption<sup>40</sup>. Both factors RANKL/OPG are synthesized by mature osteoblasts and osteoblast precursors, but inflammatory cells produce them too<sup>40</sup>. In the cascade of events, the lymphocytes are recruited and can be broadly divided into T and B populations. For instance, the T-lymphocytes secrete RANKL and IL-17 which recruit and activate osteoclasts, whereas B-lymphocytes besides dampening the inflammation, produce OPG which down-regulates osteoclasts further. Moreover, IL-17 enhances mesenchymal stem cells' anti-inflammatory activity and aid in osteoblastic maturation<sup>34</sup>. Vast literature shows that an unbalanced immune response leads to deficient fracture healing (e.g., diabetes, rheumatoid arthritis and lupus), as well as mechanical instability can perpetuate inflammation and osteolysis (e.g., inappropriate bone fixation, inadequate strain and component wear)<sup>16,26</sup>.

**Vascularity**

In another facet of our so-called hexagonal "diamond", vascularity is fundamental for healing as well (Figure 1). Angiogenesis is crucial during endochondral ossification for fracture healing and physal bone growth<sup>41</sup>. Its inhibition leads to fibrous tissue and nonunion<sup>42</sup>. Awareness in the scientific community of the VEGF pathway in endochondral and intramembranous ossification has gained popularity and is probably the most important<sup>41,43,44</sup>. Within

Fig. 1.– Progression to the hexagon-diamond model with the inclusion of osteoimmunology and vascularity. Note: IL, Interleukin; BMP, bone morphogenic protein; Ca<sub>5</sub>(PO<sub>4</sub>)<sub>3</sub>OH, hydroxyapatite; M1-M2, macrophages 1-2; RANKL/OPG, receptor activator of nuclear factor Kappa ligand/osteoprotegerin; VEGF, vascular endothelial growth factor.



the fracture hematoma, VEGF allows neovascularization in a relative injured hypoxic environment allowing soft callus formation through the delivery of trophic factors, nutrients, and osteoprogenitor cells<sup>38,45</sup>. Other factors are also implicated in angiogenesis and bone healing such as FGF, IGF, and placental-GF, which in their absence hinder fracture healing and normal bone growth<sup>45</sup>. Aside from the microenvironment, the blood supply for most long bones can be divided into periosteal and endosteal circulation, both nurturing the cortical bone (outer 1/3 and inner 2/3, respectively)<sup>46, 47</sup>. The endosteal circulation can be compromised when intramedullary fixation is performed, but this is compensated by the periosteal circulation vessels' proliferative response in the following weeks after surgery<sup>48</sup>. A metanalysis focused on the vascular anatomy of lower extremity long bones found the distal third segment to have the poorest vascular supply, and speculate that this could explain the higher nonunion rate in this region<sup>47</sup>. Hence, the importance of the zone of injury at a fracture site and the amount of soft tissue damage to the periosteum (i.e., periosteal circulation). The periosteum also provides a substrate of local trophic factors and progenitor cells<sup>49</sup>. This led to a better understanding of the importance of surgical techniques and choice of types of fixation (e.g., intramedullary versus extramedullary implants), as well as the principle of minimizing periosteal stripping during surgery<sup>49-53</sup>. For example, when convenient, the benefit of using intramedullary nailing and minimally invasive plate osteosynthesis minimize fracture exposure, and soft tissue stripping, preserving local vascularity and osteogenic/osteoinductive factors<sup>50, 51</sup>.

## Conclusion

From the aforementioned and holistic perspective, the addition of osteoimmunology and vascularity facets to the well-known 4-facet "diamond" results in a more integrative hexagon-diamond fracture healing model, mirroring the strongest inorganic structure in bone, the hydroxyapatite.

**Conflict of interest:** None to declare

## References

- Lin X, Patil S, Gao YG, Qian A. The bone extracellular matrix in bone formation and regeneration. *Front Pharmacol* 2020; 11: 757.
- Rujitanapanich S, Kumpapan P, Wanjanoi P. Synthesis of hydroxyapatite from oyster shell via precipitation. *Energy Procedia* 2014; 56: 112-7.
- Boivin G. The hydroxyapatite crystal : A closer look. *Medi-cographia* 2007; 29: 126-32.
- Tavafoghi M, Cerruti M. The role of amino acids in hydroxyapatite mineralization. *J R Soc Interface* 2016; 13: 20160462.
- Rivera-Muñoz E. Hydroxyapatite-based materials: synthesis and characterization. In Fazel-Rezai ed. *Biomedical Engineering: Frontiers and Challenges*. London: IntechOpen. 2011.
- Kay MI, Young RA, Posner AS. Crystal structure of hydroxyapatite. *Nature* 1964; 204: 1050-2.
- Zaman SU, Irfan M, Irfan M, et al. Overview of hydroxyapatite; composition, structure, synthesis methods and its biomedical uses. *Biomed Lett* 2020; 6: 84-99.
- Ramesh N, Moratti SC, Dias GJ. Hydroxyapatite-polymer biocomposites for bone regeneration: a review of current trends. *J Biomed Mater Res B Appl Biomater* 2018; 106: 2046-57.
- Prakasam M, Locs J, Salma-Ancane K, Loca D, Largeteau A, Berzina-Cimdina L. Fabrication, properties and applications of dense hydroxyapatite: a review. *J Funct Biomater* 2015; 6: 1099-140.
- Lebre F, Sridharan R, Sawkins MJ, Kelly DJ, O'Brien FJ, Lavelle EC. The shape and size of hydroxyapatite particles dictate inflammatory responses following implantation. *Sci Rep* 2017; 7: 1-13.
- Hein LE, Grassi RL, Roldan EJ, Gregori D, Varela ME, Piccinni EP. Estudios morfológicos de los cristales de hidroxiapatita tratados con pamidronato disódico. *Medicina (B Aires)* 1997; 57 (Suppl. I): 10-6.
- Martinez CA, Ozols A. Biomateriales utilizados en cirugía ortopédica como sustitutos del tejido óseo. *Rev Asoc Argent Ortop Traumatol* 2012; 77: 140-6.
- Claes L, Recknagel S, Ignatius A. Fracture healing under healthy and inflammatory conditions. *Nat Rev Rheumatol* 2012; 8: 133-43.
- Giannoudis PV, Einhorn TA, Marsh D. Fracture healing: the diamond concept. *Injury* 2007; 38 Suppl 4: 3-6.
- Andrzejowski P, Giannoudis PV. The 'diamond concept' for long bone non-union management. *J Orthop Traumatol* 2019; 20: 21.
- Foster AL, Moriarty TF, Zalavras C, et al. The influence of biomechanical stability on bone healing and fracture-related infection: the legacy of Stephan Perren. *Injury* 2021; 52: 43-52.
- Schmal H, Brix M, Bue M, et al. Nonunion - consensus from the 4th annual meeting of the danish orthopaedic trauma society. *EFORT Open Rev* 2020; 5: 46-57.
- Sinclair KL, Mafi P, Mafi R, Khan WS. The use of growth factors and mesenchymal stem cells in orthopaedics: in particular, their use in fractures and non-unions: a systematic review. *Curr Stem Cell Res Ther* 2017; 12: 312-25.
- Murri M, Smith RL, McColl K, et al. Quantifying hexagonal stacking in diamond. *Sci Rep* 2019; 9: 10334.
- Salzmann CG, Murray BJ, Shephard JJ. Extent of stacking disorder in diamond. *Diam Relat Mater* 2015; 59: 69-72.
- Ma G, Liu XY. Hydroxyapatite: hexagonal or monoclinic? *Cryst Growth Des* 2009; 9: 2991-4.
- Bulina NV., Makarova SV., Baev SG, et al. A study of thermal stability of hydroxyapatite. *Minerals* 2021; 11: 1-15.
- Zhang Q, Yang X, Li P, et al. Bioinspired engineering of honeycomb structure - Using nature to inspire human innovation. *Prog Mater Sci* 2015; 74: 332-400.
- Naqvi SM, McNamara LM. Stem cell mechanobiology and the role of biomaterials in governing mechanotransduction and matrix production for tissue regeneration. *Front Bioeng Biotechnol* 2020; 8: 597661.
- Duan ZW, Lu H. Effect of mechanical strain on cells involved in fracture healing. *Orthop Surg* 2021; 13: 369-75.

26. Guder C, Gravius S, Burger C, Wirtz DC, Schildberg FA. Osteoimmunology: A current update of the interplay between bone and the immune system. *Front Immunol* 2020; 11: 1-19.
27. Vaz K, Verma K, Protopsaltis T, Schwab F, Lonner B, Errico T. Bone grafting options for lumbar spine surgery: a review examining clinical efficacy and complications. *SAS J* 2010; 4: 75-86.
28. Lee KJH, Roper JG, Wang JC. Demineralized bone matrix and spinal arthrodesis. *Spine J*. 2005; 5: S217-S23.
29. Rihn JA, Kirkpatrick K, Albert TJ. Graft options in posterolateral and posterior interbody lumbar fusion. *Spine* 2010; 35: 1629-39.
30. Badylak SF. Decellularized allogeneic and xenogeneic tissue as a bioscaffold for regenerative medicine: Factors that influence the host response. *Ann Biomed Eng* 2014; 42: 1517-27.
31. Boden SD. Biology of lumbar spine fusion and use of bone graft substitutes: Present, future, and next generation. *Tissue Eng* 2000; 6: 383-99.
32. Nather A, David V, Teng JWH, Lee CW, Pereira BP. Effect of autologous mesenchymal stem cells on biological healing of allografts in critical-sized tibial defects simulated in adult rabbits. *Ann Acad Med Singap* 2010; 39: 599-606.
33. Zou XH, Cai HX, Yin Z, et al. A novel strategy incorporated the power of mesenchymal stem cells to allografts for segmental bone tissue engineering. *Cell Transplant* 2009; 18: 433-41.
34. Baht GS, Vi L, Alman BA. The role of the immune cells in fracture healing. *Curr Osteoporos Rep* 2018; 16: 138-45.
35. Walters G, Pountos I, Giannoudis PV. The cytokines and micro-environment of fracture haematoma: current evidence. *J Tissue Eng Regen Med* 2018; 12: 1662-77.
36. Arron JR, Choi Y. Bone versus immune system. *Nature* 2000; 408: 535-6.
37. Takayanagi H, Ogasawara K, Hida S, et al. T-cell-mediated regulation of osteoclastogenesis by signalling cross-talk between RANKL and IFN- $\gamma$ . *Nature* 2000; 408: 600-5.
38. Pountos I, Walters G, Panteli M, Einhorn TA, Giannoudis PV. Inflammatory profile and osteogenic potential of fracture haematoma in humans. *J Clin Med* 2019; 9: 47.
39. Horwood NJ. Macrophage polarization and bone formation: a review. *Clin Rev Allergy Immunol* 2016; 51: 79-86.
40. Weitzmann MN. The role of inflammatory cytokines, the RANKL/OPG axis, and the immunoskeletal interface in physiological bone turnover and osteoporosis. *Scientifica (Cairo)* 2013; 2013: 125705.
41. Keramaris NC, Calori GM, Nikolaou VS, Schemitsch EH, Giannoudis PV. Fracture vascularity and bone healing: a systematic review of the role of VEGF. *Injury* 2008; 39 (Suppl 2): 45-57.
42. Hausman MR, Schaffler MB, Majeska RJ. Prevention of fracture healing in rats by an inhibitor of angiogenesis. *Bone* 2001; 29: 560-4.
43. Gerber HP, Vu TH, Ryan AM, Kowalski J, Werb Z, Ferrara N. VEGF couples hypertrophic cartilage remodeling, ossification and angiogenesis during endochondral bone formation. *Nat Med* 1999; 5: 623-8.
44. Erickson CB, Newsom JP, Fletcher NA, et al. Anti-VEGF antibody delivered locally reduces bony bar formation following physeal injury in rats. *J Orthop Res* 2021; 39: 1658-68.
45. Watson EC, Adams RH. Biology of bone: The vasculature of the skeletal system. *Cold Spring Harb Perspect Med* 2018; 8: 031559.
46. Asghar A, Kumar A, Narayan RK, Naaz S. Is the cortical capillary renamed as the transcortical vessel in diaphyseal vascularity? *Anat Rec* 2020; 303: 2774-84.
47. Santolini E, Goumenos SD, Giannoudi M, Sanguineti F, Stella M, Giannoudis PV. Femoral and tibial blood supply: a trigger for non-union? *Injury* 2014; 45: 1665-73.
48. Greksa F, Tóth K, Boros M, Szabó A. Periosteal microvascular reorganization after tibial reaming and intramedullary nailing in rats. *J Orthop Sci* 2012; 17: 477-83.
49. Neagu TP, Țiglig M, Cocoloș I, Jecan CR. The relationship between periosteum and fracture healing. *Rom J Morphol Embryol* 2016; 57: 1215-20.
50. Whiteside LA, Ogata K, Lesker P, Reynolds FC. The acute effects of periosteal stripping and medullary reaming on regional bone blood flow. *Clin Orthop Relat Res* 1978; 131: 66-272.
51. Pape HC, Giannoudis P. The biological and physiological effects of intramedullary reaming. *J Bone Joint Surg Br* 2007; 89: 1421-6.
52. Farouk O, Krettek C, Miclau T, Schandelmaier P, Guy P, Tscherner H. Minimally invasive plate osteosynthesis and vascularity: preliminary results of a cadaver injection study. *Injury* 1997; 28Suppl 1: 7-12.
53. Kulkarni VS, Kulkarni MS, Kulkarni GS, Goyal V, Kulkarni MG. Comparison between antegrade intramedullary nailing (IMN), open reduction plate osteosynthesis (ORPO) and minimally invasive plate osteosynthesis (MIPO) in treatment of humerus diaphyseal fractures. *Injury* 2017; 48: S8-13.