

# Effect of Effective Arterial Elastance on Left Ventricular Systolic Function in Severe Valvular Aortic Stenosis

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**ABSTRACT**

**Background**

Left ventricular dysfunction in valvular aortic stenosis (AS) is related to an elevated afterload. This increase may be related to a reduction in aortic valve area (AVA), to changes in ventricular geometry and to the characteristics of the arterial vessels. Effective arterial elastance ( $E_a$ ) is an index of arterial vascular load which incorporates the characteristic arterial impedance, arterial resistance and arterial compliance.

**Objective**

To assess the effect of  $E_a$  on left ventricular systolic function in severe valvular AS.

**Material and Methods**

We prospectively studied 54 patients with severe AS; transvalvular gradient, AVA, valvular resistance and energy loss index were assessed.  $E_a$  was estimated as the end-systolic pressure/stroke volume ratio. Carotid blood pressure waveform was calibrated against blood pressure measured by conventional cuff sphygmomanometry to calculate end-systolic pressure. We estimated global afterload by the “valvulo-arterial impedance” (Zva) formulated as follows: (systolic arterial pressure + mean net pressure gradient)/stroke-volume index. Zva considers the effect of AS and  $E_a$ . Patients were divided in three groups: G1, AS with heart failure (NYHA III-IV) (n = 13), G2, symptomatic AS without heart failure (n = 13), and G3, asymptomatic AS (n = 28).

**Results**

Ejection fraction (EF) (%) was lower in G1 (33±15) compared to G2 (42±16) and to G3 (65±14); p<0.01.  $E_a$  (mm Hg/ml) and Zva (mm Hg/ml/m<sup>2</sup>) were greater in G1 (2.46±0.8 and 6.5±2.2, respectively) than in G2 and G3 (1.83±0.52 and 1.73±0.47; p<0.01, and 4.8±1.0 y 4.7±1.5; p < 0.01, respectively). When univariate analysis was performed, Zva correlated with  $E_a$  (r=0.88; p<0.0001) and EF (r=-0.41; p<0.01). In multivariate analysis  $E_a$  and Zva were independent predictors for EF.

**Conclusions**

In severe AS, the increase of the vascular component of the afterload, assessed by the  $E_a$ , contributes to a reduction in systolic function.

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**Key words** > Aortic Valve Stenosis - Left Ventricular Function - Doppler Echocardiography

<b>AVA</b>	Aortic valve area	<b>AVR</b>	Aortic valve resistance
<b><math>E_a</math></b>	Effective arterial elastance	<b>BSA</b>	Body surface area
<b>AS</b>	Aortic stenosis	<b>LVOT</b>	Left ventricular outflow tract
<b>EF</b>	Ejection fraction	<b>EDV</b>	End-diastolic volume
<b>HT</b>	Hypertension	<b>ESV</b>	End-systolic volume
<b>AMI</b>	Acute myocardial infarction	<b>LV</b>	Left ventricle
<b>ELI</b>	Energy loss index	<b>SV</b>	Stroke volume
<b>MAP</b>	Mean arterial pressure	<b>Zva</b>	Valvulo-arterial impedance
<b>ESP</b>	End-systolic pressure	<b>CO</b>	Cardiac output
<b>PP</b>	Pulse pressure		

## BACKGROUND

The presence of symptoms – angina, syncope or heart failure – along the natural history of valvular aortic stenosis (AS) is associated with high 3-year mortality (75%) in patients not submitted to surgery. (1) However, some patients without previous history of valvular heart disease, dyspnea or angina are hospitalized with congestive heart failure in functional class III-IV (NYHA). This might be due to progressive restriction in physical activity. Afterload is inversely related to myocardial fiber shortening and to left ventricular stroke volume. Thus, reduction in ejection fraction (EF) may be due to increased afterload or reduced inotropism. (2) In the latter, EF is lower than would be expected for a given level of afterload. Ventricular dysfunction in AS is generally due to excessive afterload, except in patients with significant myocardial ischemia, extensive necrosis or associated cardiomyopathy. (3) Increased afterload is a consequence of reduced aortic valve area (AVA), changes in ventricular geometry and characteristics of the arterial vessels. Therefore, in AS the relationship EF/afterload is more complex than would be expected; the sum of external factors that resist ventricular ejection, added to the effect of the obstruction of the left ventricular outflow tract, include physical characteristics of peripheral arteries, such as arterial impedance (determined by the phasic relationship between aortic pressure and aortic volume), peripheral resistance, aortic wall stiffness, (4) inertial properties of blood and properties of the reflection waves produced in arterial bifurcations. (5-7)

Recently, Briand (8) described the concept of valvulo-arterial impedance ( $Z_{va}$ ) to quantify global afterload in AS (Figure 1A). (9)  $Z_{va}$  includes the effect of valvular stenosis by energy loss index (ELI), which takes into account pressure recovery to estimate effective valve area) and arterial compliance. Although Briand found reduced EF in patients with low arterial compliance, there are other parameters that describe more accurately the hydraulic model of arterial vessels. Effective arterial elastance ( $E_a$ ) described by Sunagawa (10) is a more precise estimation of arterial vascular load, determined by the end-systolic pressure/stroke volume ratio. The goal of our study was to analyze the effect of arterial  $E_a$  on left ventricular systolic function in patients with severe valvular aortic stenosis

## MATERIAL AND METHODS

The study included 54 patients (28 men, 26 women, mean age  $71 \pm 10$  years) who prospectively underwent an echocardiographic evaluation and were found to have severe aortic valve stenosis defined as the presence of an aortic valve area  $< 1 \text{ cm}^2$ . Patients with coexisting moderate or severe aortic valve regurgitation or mitral valve regurgitation were excluded. Fifteen patients were already hospitalized; 13 of these inpatients had grade III-IV congestive heart

failure (11 coronary care unit patients and 2 general ward patients) and 2 patients had been admitted to the coronary care unit with recent onset angina. Eight patients (53%) had no previous history of aortic valve disease. The remaining 41 outpatients had been referred for assessment of an aortic systolic murmur. Symptoms were present in 13 of these patients; 5 patients complaint of angina and 8 had grade I-II dyspnea. Data collected at the time of their echocardiographic evaluation included risks factors for coronary artery disease, presence or absence of symptoms and physical examination. Blood pressure was measured in left lateral decubitus position and carotid pulse waveform was recorded. Inpatients underwent echo-Doppler once they had achieved clinical stability with medical treatment. Hypertension was considered to be present when there was a history of hypertension requiring medical therapy. Patients were considered to have significant coronary artery disease if they had one of the following criteria: 1) history of myocardial infarction, coronary angioplasty, or coronary artery bypass graft surgery; 2) a  $> 50\%$  stenosis on at least one epicardial artery on coronary angiography; and 3) a regional wall motion abnormality on echocardiogram.

### Echocardiogram and Doppler Echocardiography

Echocardiography was performed with a TOSHIBA SS140A scanner with a 2.5 MHz transducer. The patient was positioned in left lateral recumbent and electrocardiographic lead DII was used as reference. Left ventricular outflow tract (LVOT) flow was recorded in the apical five-chamber view, placing the pulsed Doppler sample volume under the aortic valve. Aortic flow was estimated with continuous wave Doppler from the apical, subxiphoid, right parasternal, and suprasternal notch views; the highest velocity detected in any imaging window was used as the peak velocity. Recordings were taken at a sweep speed of 100 mm/s. The study was recorded on a video cassette for subsequent analysis.

The following echocardiographic parameters were assessed:

- Two-dimensional echocardiography: end-diastolic volume (EDV) and end-systolic volume (ESV) were determined by area-length method in the apical 4-chamber and 2-chamber view. The aortic diameter was measured at the level of the aortic ring, Valsalva sinus, sinotubular junction and 1 cm above the sinotubular junction in the ascending aorta.
- Doppler echocardiography: Flow-time integral in the left ventricular outflow tract and aortic flow, and peak and mean transvalvular gradients using the modified Bernoulli equation were estimated.

### Calibrated Carotid Pulse Tracing

Carotid pulse tracing was recorded with a TPW – 01 A pulse transducer and blood pressure was measured in the right arm with the use of an arm-cuff sphygmomanometer in left lateral decubitus position. Carotid pulse tracing calibration was carried out according to the method used in our laboratory: (11) systolic and diastolic pressures (phase 5) are derived from the highest and lowest values on the arterial pressure trace. The distance between the maximum and minimum deflections is measured thereafter and is considered differential pressure or pulse pressure. Once pulse pressure is calculated, the distance between end-systolic point and base is measured; this is converted into mm Hg by the simple rule of three and the diastolic arterial pressure is added to it. In this way, end-systolic pressure (ESP) is determined in a non-invasive fashion.

**Assessment of Left Ventricular Systolic Function**

Ejection fraction was calculated by the conventional method.

Stroke volume (SV) was estimated as the product of flow velocity-time integral through the LVOT, and LVOT cross-section area and cardiac output (CO) as heart rate multiplied by SV.

**Assessment of Aortic Stenosis**

Effective AVA was calculated using the continuity equation (stroke volume divided by valve flow velocity-time integral).

Peak and mean aortic valve resistance (AVR) were estimated by the formula: AVR (dynes/s/ cm<sup>5</sup>) = 1.333. (Peak or mean) gradient (mm Hg)/aortic flow (ml/s). Aortic flow was determined as the ratio between SV (ml) and the left ventricular ejection time (s).

The energy loss index (ELI) was estimated. This index considers pressure recovery at the ascending aorta and is therefore more representative of the real transvalvular gradient than the gradient calculated by the continuity equation as it avoids gradient overestimation. Garcia's formula was used. (12, 13)

$$ELI \text{ (cm}^2\text{/m}^2\text{)} = [(AVA \cdot A_A) / (A_A - AVA)] / BSA$$

where A<sub>A</sub> (cm<sup>2</sup>) is the cross-sectional area of the aorta at the sino-tubular junction and BSA (cm<sup>2</sup>) corresponds to body surface area.

**Assessment of Systemic Arterial Hemodynamics**

Pulse pressure (PP) was calculated as the difference between systolic and diastolic arterial pressures measured with the use of an arm-cuff sphygmomanometer. The PP/SV ratio was estimated as an index of arterial compliance (14) and arterial elastance (E<sub>a</sub>), an adequate method to assess arterial mechanics, was determined as the ratio between ESP and SV (Figure 1 B). Calibrated carotid pulse tracing was used to calculate ESP, as it has been previously described. Systemic vascular resistance was estimated by the formula: (80 x MAP)/CO, where MAP is mean arterial pressure.

**Assessment of Global Afterload**

In patients with aortic stenosis, left ventricular afterload is determined by the degree of valvular obstruction and the

**Fig. 1. A.** Impedancia valvuloarterial (Z<sub>va</sub>). Véase explicación en el texto. PSVI: Presión sistólica del ventrículo izquierdo. PAS: Presión arterial sistémica. GMnet: Gradiente medio neto. VS: Volumen sistólico. VS<sub>i</sub>: Índice de volumen sistólico. GMvc: Gradiente medio a nivel de la vena contracta. VI: Ventrículo izquierdo. AI: Aurícula izquierda. Ao: Aorta. **B.** Registro del pulso carotídeo calibrado en simultáneo con fonocardiograma (FCG) y electrocardiograma (ECG) utilizado para el cálculo de la elastancia arterial efectiva (E<sub>a</sub>). SS: Soplo sistólico

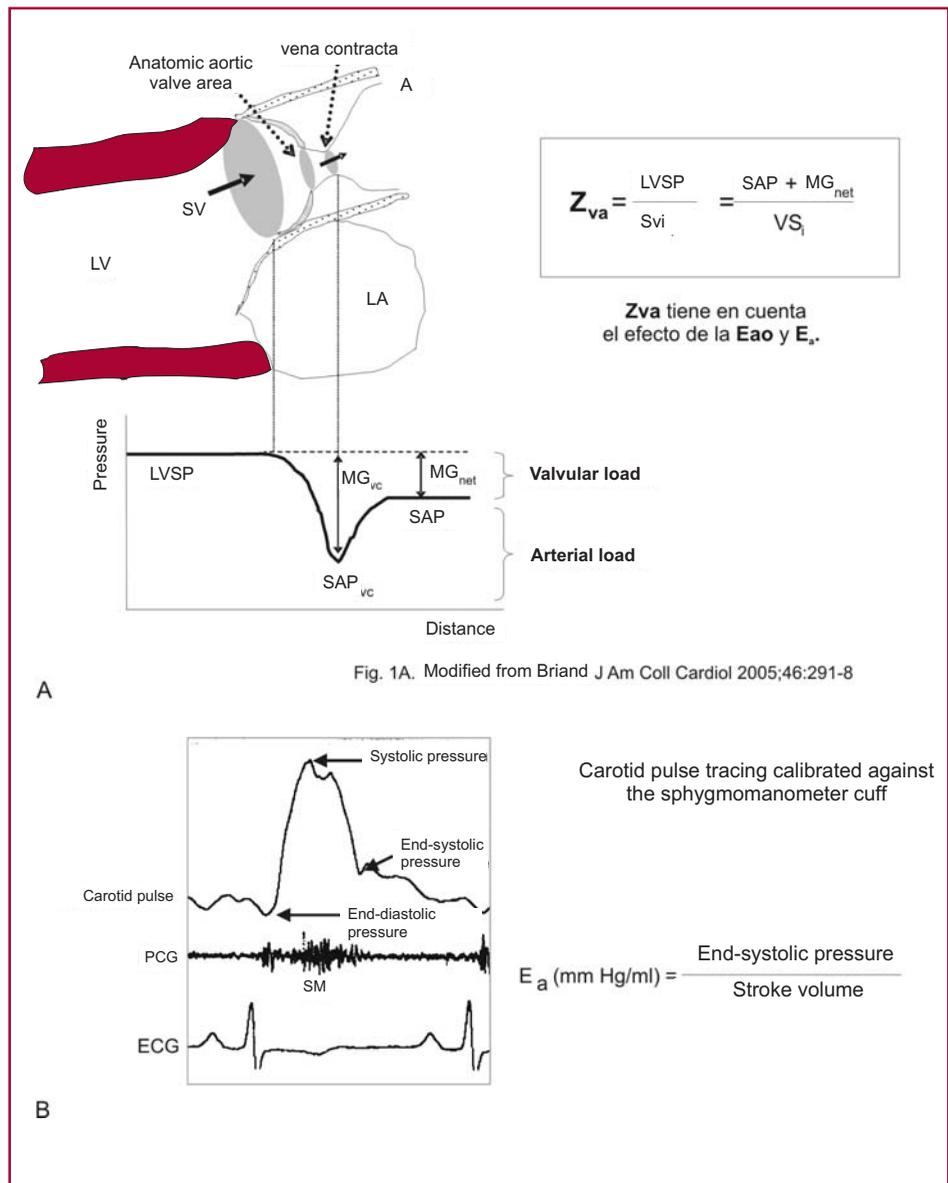


Fig. 1A. Modified from Briand J Am Coll Cardiol 2005;46:291-8

load imposed by systemic arterial system.  $Z_{va}$  was calculated using the formula (Figure 1 A):

$$Z_{va} \text{ (mm Hg/ml/m}^2\text{)} = (\text{SAP (mm Hg)} + \text{MG}_{\text{net}} \text{ (mm Hg)/SV}_i \text{ (ml/m}^2\text{)})$$

Where SAP is systemic arterial pressure,  $\text{MG}_{\text{net}}$  is the mean net pressure gradients taking into account pressure recovery according to the equation proposed by Baumgartner (15) and  $\text{SV}_i$  is SV index.

Patients were divided in three groups: group 1 (G1, n = 13) patients with grade III-IV heart failure; group 2 (G2, n = 13) patients with symptomatic aortic stenosis and group 3 (G3, n = 28) asymptomatic patients with aortic stenosis.

### Statistical analysis

Continuous variables were expressed as mean  $\pm$  standard deviation and groups were compared with analysis of variance. Univariate analysis was performed using the coefficient of correlation ( $r$ ). Forward stepwise multivariate analysis was used to establish independent predictors of EF. A  $p$  value  $< 0.05$  was considered statistically significant.

## RESULTS

Table 1 shows the demographic and clinical characteristics of the study population. The distribution of age, body surface area and sex was similar among groups; however, the proportion of men was higher in groups 1 and 2. The prevalence of risk factors -hypertension, smoking habits, dyslipemia and obesity- was similar in the three groups. History of coronary heart disease was more frequent in patients in groups 1 and 2. By definition, grade III-IV dyspnea was present in the 13 patients in G1, and 4 of them also had angina. Eight patients in G2 complaint of grade I-II dyspnea, and angina was present in 5 patients.

### Systemic Arterial Hemodynamics (Table 2)

There were no significant differences among the three groups in systolic arterial pressure, diastolic arterial pressure, end-systolic pressure and heart rate. Pulse pressure, a clinical parameter that estimates arterial compliance, was also similar in the three groups.  $E_a$  was significantly greater in G1 ( $2.46 \pm 0.8$  mm Hg/ml) compared to G2 and G3 ( $1.83 \pm 0.52$  mm Hg/ml and  $1.73 \pm 0.47$  mm Hg/ml, respectively;  $p < 0.01$ ). PP/SV ratio was greater in G1 ( $1.1 \pm 0.41$ ;  $p < 0.03$ ) and G2 ( $0.94 \pm 0.33$ ;  $p < 0.03$ ) than in G3. This last finding was influenced by the reduction in SV in G1 and G2 ( $49 \pm 18$  ml and  $55 \pm 19$  ml  $p < 0.03$ ) compared to G3 ( $69 \pm 18$  ml), due to the fact that stroke volume is the denominator in the PP/SV ratio. These findings suggest that in patients in groups 1 and 2 PP does not represent a reduction in arterial compliance as a decreased SV might mask such finding.

### Left Ventricular Systolic Function

As it was expected, EF was significantly reduced in G1 ( $33\% \pm 15\%$ ) compared to G2 and G3 ( $42\% \pm 16\%$  and  $65\% \pm 14\%$ ;  $p < 0.01$ ). Ejection fraction was lower in G2 than in G3; however, this difference was not significant.

### Severity of Aortic Stenosis

Values of aortic valve area, peak and mean valvular resistance and ELI did not differ among groups. Although peak gradient ( $62 \pm 21$  mm Hg) and mean gradient ( $30 \pm 13$  mm Hg) were significantly lower in G1 compared to G2 ( $77 \pm 36$  mm Hg and  $37 \pm 22$  mm Hg) and G3 ( $77 \pm 29$  mm Hg and  $46 \pm 18$  mm Hg), this difference was not significant.

**Table 1.** Demographic and clinical characteristics

	Group 1 (n = 13)	Group 2 (n = 13)	Group 3 (n = 28)
Sex, n			
Male	8	9	14
Female	5	4	14
Age (years)	68 $\pm$ 14	68 $\pm$ 9	70 $\pm$ 11
Body surface area (m <sup>2</sup> )	1.87 $\pm$ 0.19	1.83 $\pm$ 0.19	1.83 $\pm$ 0.23
Comorbidities and risk factors (%)			
Coronary artery disease	30	20	0
Previous myocardial infarction	20	20	20
Hypertension	100	100	78
Dyslipemia	43	25	12
Diabetes mellitus	28	0	33
Smoking habits	57	100	22
Obesity	43	0	22
Symptoms			
Grade I-II dyspnea	0	8	0
Grade III-IV dyspnea	13	0	0
Angina	4	5	0

	Group 1 (n = 13)	Group 2 (n = 13)	Group 3 (n = 28)
Systemic arterial pressure			
Systolic arterial pressure (mm Hg)	123 ± 18	124 ± 24	130 ± 20
Diastolic arterial pressure (mm Hg)	75 ± 9	75 ± 14	83 ± 11
Pulse pressure (mm Hg)	48 ± 17	48 ± 13	47 ± 16
End-systolic pressure (mm Hg)	92 ± 14	93 ± 14	97 ± 13
Heart rate (bpm)	76 ± 12	73 ± 11	69 ± 18
E <sub>a</sub> (mm Hg/ml)	2.46 ± 0.8 *	1.83 ± 0.52	1.73 ± 0.47
PP/SV	1.1 ± 0.41 <sup>†</sup>	0.94 ± 0.33 <sup>‡</sup>	0.73 ± 0.31
Systemic vascular resistance (dyne/s/cm <sup>5</sup> )	2.163 ± 742	1.948 ± 764	1.696 ± 480
SV (ml)	49 ± 18 <sup>†</sup>	55 ± 19 <sup>†</sup>	69 ± 18
Cardiac output (L/min)	4 ± 1.2	4.2 ± 1.5	4.4 ± 2
Aortic flow (ml/s)	172 ± 44	176 ± 51	192 ± 51
EF (%)	33 ± 15 *	42 ± 16	65 ± 14
AVA (cm <sup>2</sup> )	0.61 ± 0.22	0.58 ± 0.20	0.67 ± 0.18
Peak gradient (mm Hg)	62 ± 21	77 ± 36	77 ± 29
Mean gradient (mm Hg)	30 ± 13	37 ± 22	46 ± 18
Peak valvular resistance (dyne/s/cm <sup>5</sup> )	565 ± 282	650 ± 293	557 ± 209
Mean valvular resistance (dyne/s/cm <sup>5</sup> )	290 ± 84	391 ± 184	317 ± 140
Energy loss index (cm <sup>2</sup> /m <sup>2</sup> )	0.39 ± 0.16	0.36 ± 0.14	0.40 ± 0.13
Zva (mm Hg/ml/m <sup>2</sup> )	6.5 ± 2.2 *	4.8 ± 1.0	4.7 ± 1.5

\* p < 0.01 G1 versus G2 and G3; † p < 0.03 G1 versus G2 and G3; ‡ p < 0.03 G2 versus G3.

E<sub>a</sub>: Effective arterial elastance PP: Pulse pressure. SV: Stroke volume. EF: Ejection fraction. AVA: Aortic valve area. Zva: Valvulo-arterial impedance.

**Table 2.** Systemic arterial hemodynamics

### Global Afterload

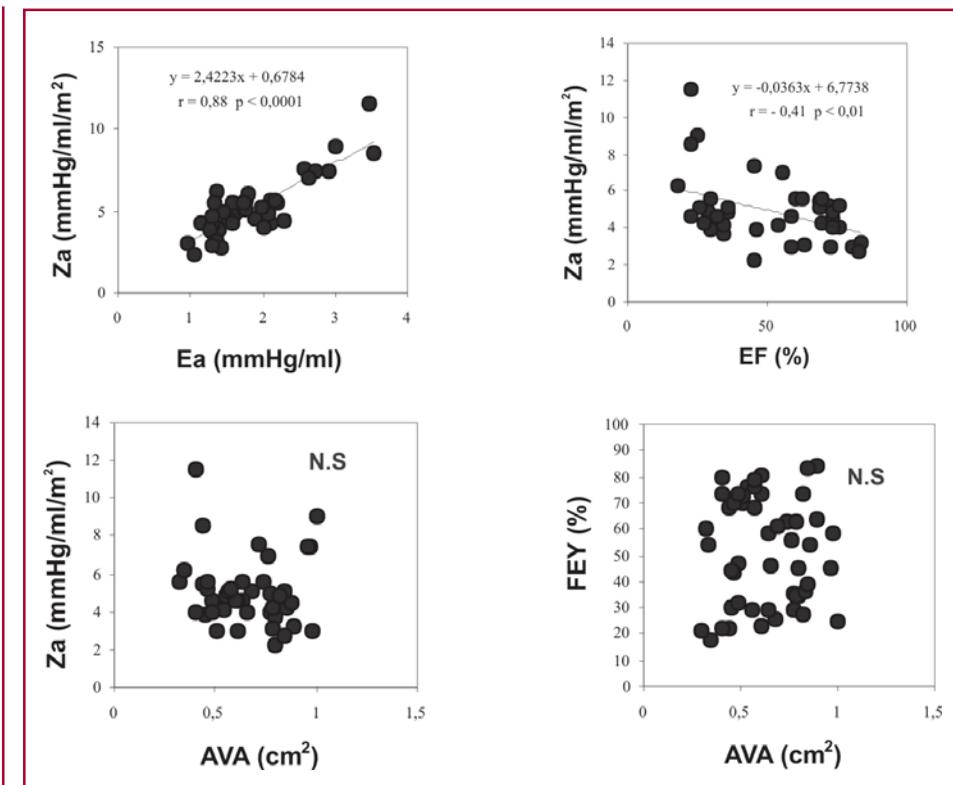
Zva was greater in G1 ( $6.5 \pm 2.2$  mm Hg/ml/m<sup>2</sup>) than in G2 and G3 ( $4.8 \pm 1$  mm Hg/ml/m<sup>2</sup> and  $4.7 \pm 1.5$  mm Hg/ml/m<sup>2</sup>, respectively; p < 0.01) and had a significant correlation with E<sub>a</sub> (r = 0.88; p < 0.0001, y = 2.4223x + 0.6784) and EF (r = - 0.41; p < 0.01 y = - 0.0363x + 6.7738) (Figure 2). No correlation was observed between Zva and AVA or EF and AVA (figure 2). At multivariate analysis, E<sub>a</sub> and Zva were independent predictors of EF (coefficient -4.25 T 2.36; p < 0.02).

### DISCUSSION

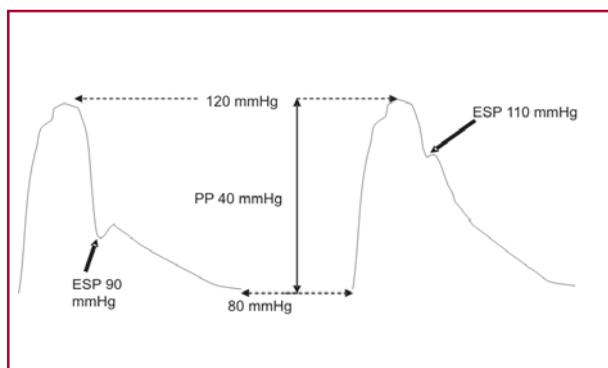
The effect of E<sub>a</sub> on global afterload (Zva) and EF in patients with severe aortic stenosis is the main finding of this study, which has potential prognostic and therapeutic implications taking into account that, until recently, surgery was the only therapeutic option. (16) For the purpose of the analysis, patients were divided in three groups, resembling the natural history of severe AS: asymptomatic and compensated patients were included in G3 group; intermediate symptomatic patients were represented by G2, and patients in G1 presented decompensated heart failure. Nevertheless, most patients with heart failure were not aware they had aortic stenosis, probably attributed to progressive reduction in their physical activities and/or absence of early diagnosis. Ejection

fraction is inversely related to afterload, but in AS this relationship is more complex due to difficulties in estimating the contribution of ventricular outflow tract obstruction and ventricular/vascular coupling to increased afterload. (9) In patients with AS, increased blood pressure associated with isometric exercise, phenylephrine (17) or angiotensin II (18) causes a reduction in stroke volume and increases left ventricular end-diastolic pressure; in addition, symptoms may be present in patients with hypertension associated with AS with less reduced aortic valve area and lower transvalvular aortic gradients. (19) Severity of AS, compared through transvalvular flow, AVA, peak and mean aortic resistance and ELI, was similar in the three groups, therefore valvular "load" may be considered identical. Peak and mean transvalvular gradients were lower in G1, but this difference was not statistically significant, probably due to reduced SV and transvalvular volume flow rate observed in this group. E<sub>a</sub> was significantly greater in patients with heart failure, showing a negative correlation with EF. PP/SV ratio was higher in G1 and G2; nevertheless, this parameter did not show any significant correlation with EF. PP/SV ratio, an index of arterial compliance (20) might have been influenced by the reduction in SV seen in those groups. E<sub>a</sub> seems to be more adequate than PP/SV ratio for the assessment of arterial mechanics as it incorporates characteristic impedance (Z<sub>0</sub>), resistance (R), arterial compliance (C)

**Fig. 2.** Correlación de la impedancia valvuloarterial ( $Z_{va}$ ) con la elastancia arterial efectiva ( $E_a$ ) y la fracción de eyección ( $F_{ey}$ ) (superior) y del área valvular aórtica (AVA) con la impedancia valvuloarterial ( $Z_{va}$ ) y la fracción de eyección ( $F_{ey}$ ) (inferior).



and cardiac cycle length (T). (21) Both indices share the same denominator (SV); however end-systolic pressure used by  $E_a$  is more accurate to characterize vascular load than pulse pressure (used in PP/SV ratio), (10) as R/T contributes 2.5 times more to  $E_a$  than 1/C. (22) Resistance is normalized to cardiac cycle length in R/T ratio; thus this index considers both pulsatile and static (R) blood pressure components. Figure 3 shows that two patients may present the same values of systolic arterial pressure, diastolic arterial pressure and PP but different values of ESP, indicating diverse arterial elastances. (22) According to our findings, vascular “load” was significantly increased in G1 patients, in accordance with increased  $Z_{va}$ , a parameter that evaluates global afterload in AS.  $Z_{va}$  significantly correlated with  $E_a$ , but not with PP/SV. Briand (8) studied patients with moderate and severe AS who were classified in different groups according to arterial stiffness (normal or increased) determined by PP/SV. He reported that PP/SV ratio had a significant impact on EF. Unlike Briand’s study, we classified our patients with AS in three groups in an attempt to mimic the natural history of the disease. Even more, the concept of  $E_a$  seems more accurate than PP/SV to characterize arterial properties. (24) As Briand, we also found a high incidence of cardiovascular risk factors, such as hypertension, smoking habits, dyslipemia and obesity in all the groups, especially in G2 and G3, which might probably pose a nega-



**Fig. 3.** Véase explicación en el texto.

tive influence in the physical properties of the arterial system. Therefore, this finding widens the possibilities of medical treatment of AS, (19, 25, 26) an active process, which requires similar therapy for risk factors as patients with coronary artery disease, especially in early stages of the disease (mild to moderate aortic stenosis). These therapeutic measurements are not opposed to treatment with statins to reduce AS progression, (27) as aortic valve disease and vascular atherosclerosis present similar pathophysiological changes which include lipid infiltration, neoangiogenesis and calcification. (29) However,

statins failed to produce any benefit in some studies. (28) Reduction of arterial vascular load is clinically relevant in patients with severe AS, EF < 35% and cardiac index < 2.2 L/min/m<sup>2</sup>; treatment with sodium nitroprusside before aortic valve replacement improves the hemodynamic profile of these patients. (30, 31)

### Study Limitations

This study failed to establish the precise influence of coronary artery disease on left ventricular function, as coronary arteriography was not performed to most patients due to absence of indication (52% of patients were asymptomatic) or to the fact that data from patients in groups 1 and 2 was not completely available.

### CONCLUSIONS

In severe AS, the increase of the vascular component of the afterload, assessed by the E<sub>a</sub>, contributes to a reduction in systolic function.

### RESUMEN

#### Efecto de la elastancia arterial efectiva sobre la función sistólica ventricular izquierda en la estenosis aórtica grave

##### Antecedentes

La disfunción ventricular izquierda en la estenosis aórtica (EAo) está relacionada con el exceso de poscarga. El aumento de la poscarga puede deberse a la reducción del área valvular aórtica (AVA), a cambios en la geometría ventricular y a las características de la vasculatura arterial. La elastancia arterial efectiva (E<sub>a</sub>) es un índice de carga vascular que incorpora la impedancia característica, la resistencia y la distensibilidad arterial.

##### Objetivo

Evaluar el efecto de la E<sub>a</sub> sobre la función sistólica del ventrículo izquierdo en la EAo grave.

##### Material y métodos

Se estudiaron prospectivamente 54 pacientes con EAo grave evaluados mediante los gradientes transvalvulares, el AVA, la resistencia valvular y el índice de pérdida de energía. La E<sub>a</sub> se calculó mediante el cociente entre la presión de fin de sístole y el volumen sistólico. La presión de fin de sístole se obtuvo a partir del pulso carotídeo calibrado con la presión arterial medida con esfigmomanómetro. Como medida de la poscarga global, se calculó la impedancia valvuloaórtica (Z<sub>va</sub>), definida por: (presión sistólica + gradiente medio neto) / índice de volumen sistólico. La Z<sub>va</sub> tiene en cuenta el efecto de la EAo y la E<sub>a</sub>. Los pacientes se dividieron en tres grupos: G1, EAo con insuficiencia cardíaca (NYHA III-IV) (n = 13), G2, EAo sintomática pero sin insuficiencia cardíaca (n = 13) y G3, EAo asintomática (n = 28).

##### Resultados

La fracción de eyección (Fey) (%) fue menor en el G1 (33 ± 15) en comparación con el G2 (42 ± 16) y el G3 (65 ± 14); p < 0,01. La E<sub>a</sub> (mm Hg/ml) fue mayor en el G1 (2,46 ± 0,8) con respecto al G2 y el G3 (1,83 ± 0,52 y 1,73 ± 0,47; p < 0,01), al igual que la Z<sub>va</sub> (mm Hg/ml/m<sup>2</sup>): G1 (6,5 ± 2,2), G2

y G3 (4,8 ± 1,0 y 4,7 ± 1,5; p < 0,01). En el análisis univariado, la Z<sub>va</sub> se correlacionó con la E<sub>a</sub> (r = 0,88; p < 0,0001) y la Fey (r = -0,41; p < 0,01). En el análisis multivariado, la E<sub>a</sub> y la Z<sub>va</sub> fueron predictores independientes de la fracción de eyección.

### Conclusión

En la EAo grave, el aumento del componente vascular de la poscarga evaluado a través de la E<sub>a</sub> contribuye a la reducción de la función sistólica.

**Palabras clave** > Estenosis de la válvula aórtica - Función ventricular izquierda - Ecocardiografía de Doppler

### BIBLIOGRAPHY

1. Frank S, Johnson A, Ross J Jr. Natural history of valvular aortic stenosis. *Br Heart J* 1973;35:41-6.
2. Migliore RA. Manejo terapéutico de la estenosis aórtica severa: ¿Cuándo es demasiado tarde el reemplazo valvular aórtico? *Rev Soc Parag Cardiol* 2004;2:76-82.
3. Migliore RA. Estenosis aórtica. En: Piñeiro DJ. *Ecocardiografía para la toma de decisiones clínicas*. Buenos Aires: Editorial Médica Panamericana; 2005. p. 529-67.
4. Stergiopoulos N, Westerhof N. Determinants of pulse pressure. *Hypertension* 1998;32:556-9.
5. Nichols WW, Conti CR, Walker WE, Milnor WR. Input impedance of the systemic circulation in man. *Circ Res* 1977;40:451-8.
6. Nichols WW, O'Rourke MF. Wave reflection. En: Nichols WW, O'Rourke MF. *Mc Donald's blood flow in arteries. Theoretical, experimental and clinical principles*. 4<sup>th</sup> ed. NY, Oxford University Press; 1998. p. 201.
7. Stergiopoulos N, Westerhof BE, Westerhof N. Total arterial inertance as the fourth element of the windkessel model. *Am J Physiol* 1999;276:H81-8.
8. Briand M, Dumesnil JG, Kadem L, Tongue AG, Rieu R, Garcia D, et al. Reduced systemic arterial compliance impacts significantly on left ventricular afterload and function in aortic stenosis: implications for diagnosis and treatment. *J Am Coll Cardiol* 2005;46:291-8.
9. Garcia D, Barenbrug PJ, Pibarot P, Dekker AL, van der Veen FH, Maessen JG, et al. A ventricular-vascular coupling model in presence of aortic stenosis. *Am J Physiol Heart Circ Physiol* 2005;288:H1874-84.
10. Sunagawa K, Maughan WL, Burkoff D, Sagawa K. Left ventricular interaction with arterial load studied in isolated canine ventricle. *Am J Physiol* 1983;245:H773-80.
11. Migliore RA, Guerrero FT, Adaniya ME, Ianariello J, Tamagusuku H, Posse RA. Estimación de la pre y poscarga ventricular izquierda en la enfermedad de Chagas. *Rev Argent Cardiol* 1990;58:252-9.
12. Garcia D, Pibarot P, Dumesnil JG, Sakr F, Durand LG. Assessment of aortic valve stenosis severity: A new index based on the energy loss concept. *Circulation* 2000;101:765-71.
13. Garcia D, Dumesnil JG, Durand LG, Kadem L, Pibarot P. Discrepancies between catheter and Doppler estimates of valve effective orifice area can be predicted from the pressure recovery phenomenon: practical implications with regard to quantification of aortic stenosis severity. *J Am Coll Cardiol* 2003;41:435-42.
14. Chemla D, Hébert JL, Coirault C, Zamani K, Suard I, Colin P, et al. Total arterial compliance estimated by stroke volume-to-aortic pulse pressure ratio in humans. *Am J Physiol* 1998;274:H500-5.
15. Baumgartner H, Stefenelli T, Niederberger J, Schima H, Maurer G. Overestimation of catheter gradients by Doppler ultrasound in patients with aortic stenosis: a predictable manifestation of pressure recovery. *J Am Coll Cardiol* 1999;33:1655-61.
16. Chan KL. Is aortic stenosis a preventable disease? *J Am Coll Cardiol* 2003;42:593-9.
17. Awan N, Vismara LA, Miller RR, DeMaria AN, Mason DT. Effects of isometric exercise and increased arterial impedance on left ven-

- tricular function in severe aortic valvular stenosis. *Br Heart J* 1977;39:651-6.
18. Perloff JK, Binnion PF, Caulfield WH, DeLeon AC Jr. The use of angiotensin in the assessment of left ventricular function in fixed orifice aortic stenosis. *Circulation* 1967;35:347-57.
19. Antonini-Canterin F, Huang G, Cervesato E, Faggiano P, Pavan D, Piazza R, et al. Symptomatic aortic stenosis: does systemic hypertension play an additional role? *Hypertension* 2003;41:1268-72.
20. Stergiopoulos N, Segers P, Westerhof N. Use of pulse pressure method for estimating total arterial compliance in vivo. *Am J Physiol* 1999;276:H424-8.
21. Segers P, Stergiopoulos N, Westerhof N. Relation of effective arterial elastance to arterial system properties. *Am J Physiol Heart Circ Physiol* 2002;282:H1041-6.
22. Chemla D, Antony I, Lecarpentier Y, Nitenberg A. Contribution of systemic vascular resistance and total arterial compliance to effective arterial elastance in humans. *Am J Physiol Heart Circ Physiol* 2003;285:H614-20.
23. Kelly RP, Ting CT, Yang TM, Liu CP, Maughan WL, Chang MS, et al. Effective arterial elastance as index of arterial vascular load in humans. *Circulation* 1992;86:513-21.
24. Peterson KL. Severe calcific aortic stenosis left ventricular afterload and its quantification. *J Am Coll Cardiol* 2005;46:299-301.
25. Volberg VI, Berensztein CS, Ber MG, Lanosa G, Lerman J, Piñeiro DJ. Eficacia de la relación gradiente pico-gradiente medio para el diagnóstico de la gravedad de la estenosis aórtica. *Rev Argent Cardiol* 2006;74:123-8.
26. Chambers J. Can high blood pressure mask severe aortic stenosis? *J Heart Valve Disease* 1998;7:277-8.
27. Moura LM, Ramos SF, Zamorano JL, Barros IM, Azevedo LF, Rocha-Gonçalves F, et al. Rosuvastatin affecting aortic valve endothelium to slow the progression of aortic stenosis. *J Am Coll Cardiol* 2007;49:554-61.
28. Cowell SJ, Newby DE, Prescott RJ, Bloomfield P, Reid J, Northridge DB, et al; Scottish Aortic Stenosis and Lipid Lowering Trial, Impact on Regression (SALTIRE) Investigators. A randomized trial of intensive lipid-lowering therapy in calcific aortic stenosis. *N Engl J Med* 2005;352:2389-97.
29. Mohler ER 3rd, Gannon F, Reynolds C, Zimmerman R, Keane MG, Kaplan FS. Bone formation and inflammation in cardiac valves. *Circulation* 2001;103:1522-8.
30. Khot UN, Novaro GM, Popoviæ ZB, Mills RM, Thomas JD, Tuzcu EM, et al. Nitroprusside in critically ill patients with left ventricular dysfunction and aortic stenosis. *N Engl J Med* 2003;348:1756-63.
31. Popovic ZB, Khot UN, Novaro GM, Casas F, Greenberg NL, Garcia MJ, et al. Effects of sodium nitroprusside in aortic stenosis associated with severe heart failure: pressure-volume loop analysis using a numerical model. *Am J Physiol Heart Circ Physiol* 2005;288:H416-23.